

# Package ‘rsleep’

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**Type** Package

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**License** MIT + file LICENSE

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a7

*A7 spindle detection algorithm*


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## Description

A sleep spindle detection algorithm that emulates human expert spindle scoring

**Usage**

```

a7(
  x,
  sRate,
  window = 0.3,
  step = 0.1,
  butter_order = 5,
  A7absSigPow = 1.25,
  A7relSigPow = 1.6,
  A7sigmaCov = 1.3,
  A7sigmaCorr = 0.69
)

```

**Arguments**

x	EEG signal in uV.
sRate	Sample rate of the signal.
window	Size of the window in seconds. Default: 0.3
step	Size of the step between windows in seconds. Default: 0.1
butter_order	Order of the Butterworth filters. Default: 5
A7absSigPow	A7absSigPow threshold. Default: 1.25
A7relSigPow	A7relSigPow threshold. Default: 1.6
A7sigmaCov	A7sigmaCov threshold. Default: 1.3
A7sigmaCorr	A7sigmaCorr threshold. Default: 0.69

**Details**

A sleep spindle detection algorithm based on 4 features computed along segmented signal according to 'window' size and 'step' size parameters.

1. Absolute sigma power

$$A7absSigPow = \log_{10} \left( \sum_{i=1}^N \frac{EEG\sigma_i^2}{N} \right)$$

2. Relative sigma power

$$A7relSigPow = zscore \left( \log_{10} \left( \frac{PSA_{11-16Hz}}{PSA_{4.5-30Hz}} \right) \right)$$

3. Sigma covariance

$$A7sigmaCov = zscore \left( \log_{10} \left( \frac{1}{N} \sum_{i=1}^N (EEG_{bf_i} - \mu_{EEG_{bf}}) (EEG_{\sigma_i} - \mu_{EEG_{\sigma}}) \right) \right)$$

4. Sigma correlation

$$A7sigmaCorr = \frac{\text{cov}(EEG_{bf}, EEG_{\sigma})}{sd_{EEG_{bf}} * sd_{EEG_{\sigma}}}$$

**Value**

Detected spindles and associated features.

**References**

Lacourse, K., Delfrate, J., Beaudry, J., Peppard, P., & Warby, S. C. (2019). A sleep spindle detection algorithm that emulates human expert spindle scoring. In *Journal of Neuroscience Methods* (Vol. 316, pp. 3–11). Elsevier BV. <https://doi.org/10.1016/j.jneumeth.2018.08.014>

**Examples**

```
tryCatch({
  fpath <- paste0(tempdir(),"c3m2_n2_200hz_uv.csv")

  download.file(
    url = "https://rsleep.org/data/c3m2_n2_200hz_uv.csv",
    destfile = fpath)

  # Read only a sample of the EEG signal
  s = read.csv(fpath,header = FALSE)[,1][25000:45000]

  file.remove(fpath)

  a7_results = a7(s, 200)

  # Plot the first detected spindle
  data = data.frame(x=s,index=seq_along(s))
  a = a7_results$spindles$idxCStart[1]
  b = a7_results$spindles$idxCEnd[1]
  data = data[(data$index <= (b+600)) & (data$index >= (a-600)), ]
  library(ggplot2)
  ggplot(data, aes(x = index, y = x)) +
    geom_line() +
    geom_line(data = subset(data, index >= a & index <= b), aes(x = index, y = x), color = "red") +
    labs(x = "Signal index", y = "C3-M2") +
    theme_minimal()

  # Visualise features distribution

  hist(a7_results$df$absSigPow,main = "A7absSigPow")

  hist(a7_results$df$relSigPow,main = "A7relSigPow")

  hist(a7_results$df$sigmaCov,main = "A7sigmaCov")

  hist(a7_results$df$sigmaCorr,main = "A7sigmaCorr")
}, error = function(e) {
  print("Error executing this example, check your internet connection.")
})
```

**Description**

This function implements an adaptive normalization method on a given respiratory signal.

**Usage**

adanorm(x, sRate)

**Arguments**

x                      Numeric vector representing the input signal to be normalized.  
sRate                  Integer value representing the sampling rate of the signal (number of samples per second).

**Details**

It is designed to preserve the parts of the signal where the amplitude of respiration is small, typically when the body maintains a sleeping posture for extended periods.

Adaptive normalization first segments the signal into 1 second window before computing  $A(k)$  and is based on the following equations:

Equation (1) - Mean absolute deviation:

$$A(k) = \frac{1}{f_s} \sum_{i=k \cdot f_s}^{(k+1) \cdot f_s - 1} |x(i)|$$

Equation (2) - Standard deviation:

$$\sigma(k) = \sqrt{\frac{1}{f_s - 1} \sum_{i=k \cdot f_s}^{(k+1) \cdot f_s - 1} (x(i) - \bar{x}(k))^2}$$

Equation (3) - Adaptive normalization factor, initialized to 1.

$$F_{\text{norm}}(k) = \min(0.95F_{\text{norm}}(k-1) + 0.05A(k), 0.95F_{\text{norm}}(k-1) + 0.05\sigma(k))$$

**Value**

Numeric vector representing the adaptively normalized signal.

**References**

Choi, S. H., Yoon, H., Kim, H. S., Kim, H. B., Kwon, H. B., Oh, S. M., Lee, Y. J., & Park, K. S. (2018). Real-time apnea-hypopnea event detection during sleep by convolutional neural networks. In *Computers in Biology and Medicine* (Vol. 100, pp. 123–131). Elsevier BV. <https://doi.org/10.1016/j.combiomed.2018.06>

---

bandpass

*Bandpass Filter Function*

---

### Description

This function applies a bandpass filter to a signal. It first normalizes the high and low frequencies based on the Nyquist frequency, then creates a Butterworth filter using the ‘`signal::butter`’ function, and finally applies the filter to the signal using ‘`signal::filtfilt`’.

### Usage

```
bandpass(x, high, low, sRate, order = 5)
```

### Arguments

<code>x</code>	A numeric vector representing the signal to be filtered.
<code>high</code>	The high cutoff frequency for the bandpass filter.
<code>low</code>	The low cutoff frequency for the bandpass filter.
<code>sRate</code>	The sampling rate of the signal.
<code>order</code>	The order of the Butterworth filter, defaulting to 5.

### Value

A numeric vector representing the filtered signal.

### References

If applicable, add references here.

### See Also

[butter](#), [filtfilt](#)

### Examples

```
sample_signal <- sin(seq(0, 10, length.out = 1000))
filtered_signal <- bandpass(sample_signal, high = 0.3, low = 0.1, sRate = 100)
```

---

bands_psd	<i>Compute power spectral density of bands listed in the bands argument.</i>
-----------	--

---

### Description

'bands\_psd' calculates power spectral densities estimates on bands. Bands are computed from spectrogram bands equal or greater than lower limit and inferior to the upper limit.

### Usage

```
bands_psd(signal, sRate, bands, normalize = FALSE, method = "pwelch")
```

### Arguments

signal	Numerical vector of the signal.
sRate	Signal sample rate in Hertz.
bands	A list of bands to compute with lower and upper limits in the form 'list(c(0,4),c(4,8))'
normalize	A band to normalize (divide) by. Defaults to 'c(0.5,40)'. Can be set up to FALSE for raw results. Defaults to FALSE.
method	Character. Method to use to compute power spectral density. "pwelch" or "psm". Defaults to "pwelch".

### Value

A list of bands powers.

### Examples

```
signal <- sin(seq(0,100,0.01))
bands_psd(bands = list(c(0,4),c(4,8)), signal = signal, sRate = 200)
```

---

chambon2018	<i>Deep Learning Architecture for Temporal Sleep Stage Classification model implementation in Keras.</i>
-------------	--

---

### Description

Keras implementation of the deep learning architecture described by Chambon & AI in "A Deep Learning Architecture for Temporal Sleep Stage Classification Using Multivariate and Multimodal Time Series". Consecutives polysomnography (PSG) epochs are supposed to be input to the model to fit on categorized stages as output. 'write\_batches\_psg()' function writes files batches with the right format for 'x' and 'y' values. The model can then be trained using the 'train\_batches()' function. 'score\_psg()' uses this model to predict PSG epochs from a raw European Data Format (EDF) record.

**Usage**

```
chambon2018(channels = 6, samples = 6300)
```

**Arguments**

channels            Integer. Number of channels in each input.  
 samples            Integer. Number of samples in each channel.

**Value**

A Keras sequential model.

**References**

Chambon, S., Galtier, M., Arnal, P., Wainrib, G. and Gramfort, A. (2018) A Deep Learning Architecture for Temporal Sleep Stage Classification Using Multivariate and Multimodal Time Series. IEEE Trans. on Neural Systems and Rehabilitation Engineering 26:(758-769).

---

check_events	<i>Check events dataframe format compliance.</i>
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---

**Description**

Check events dataframe format compliance.

**Usage**

```
check_events(events)
```

**Arguments**

events            Events dataframe. Dataframe must contain begin (POSIXt), end (POSIXt) and event (character) columns.

**Value**

Boolean, according to the events dataframe format compliance.

**Examples**

```
events <- data.frame(begin = as.POSIXct(c(1536967800, 1536967830, 1536967860), origin = "1970-01-01"))
events$end <- as.POSIXct(c(1536967830, 1536967860, 1536967890), origin = "1970-01-01")
events$event = c("N3", "N3", "REM")
rsleep::check_events(events)
```



---

choi2018	<i>Convolutional neural network for real-time apnea-hypopnea event detection during sleep</i>
----------	---

---

**Description**

Keras implementation of the deep learning architecture described by Choi & Al in "Real-time apnea-hypopnea event detection during sleep by convolutional neural network".

**Usage**

```
choi2018(segment_size = 160)
```

**Arguments**

`segment_size` Integer. The size of the segment to predict.

**Value**

A Keras sequential model.

**References**

Choi SH, Yoon H, Kim HS, et al. Real-time apnea-hypopnea event detection during sleep by convolutional neural networks. *Computers in Biology and Medicine*. 2018;100:123-131.

---

ckappa	<i>Computes Cohen's Kappa for agreement in the case of 2 raters.</i>
--------	--

---

**Description**

Cohen's kappa coefficient value is a robust statistical measure of inter-rater agreement published in 1960 by Jacob Cohen. It has been reused by numerous studies in sleep medicine to measure the accuracy of predictions, especially for automatic sleep staging.

**Usage**

```
ckappa(observed, predicted)
```

**Arguments**

`observed` The vector of observed values (truth).  
`predicted` The vector of predicted values.

## References

Cohen J. A Coefficient of Agreement for Nominal Scales. Educational and Psychological Measurement. 1960;20:37-46.

## Examples

```
observed = c("AWA", "N1", "N2", "N3", "REM")
predicted = c("AWA", "AWA", "N2", "N3", "REM")
ckappa(observed, predicted)
```

---

clean_oximetry	<i>Clean Oximetry Signal</i>
----------------	------------------------------

---

## Description

This function processes an oximetry signal vector to remove values below a specified threshold. It is designed to enhance the quality of oximetry data by replacing sub-threshold impossible values with the nearest valid data points.

## Usage

```
clean_oximetry(oximetry, threshold = 70)
```

## Arguments

oximetry	A numeric vector representing the oximetry signal. Each element corresponds to an oximetry reading.
threshold	A numeric value setting the minimum acceptable oximetry value. Default is 70. Values in 'oximetry' below this threshold will be replaced with the nearest value above the threshold or an average of the nearest valid values on either side.

## Details

The function iterates through the 'oximetry' vector. For each value below the 'threshold', it searches for the nearest valid value (above the threshold) to the left and right. If both neighbors are found, it replaces the sub-threshold value with their average. If only one valid neighbor is found, it uses that value.

The algorithm ensures that the processed signal retains the general pattern of the original data while mitigating the impact of anomalously low readings.

## Value

A numeric vector of the same length as 'oximetry'. Sub-threshold values are replaced based on nearby valid readings.

**Examples**

```
oximetry_data <- c(91, 92, 91, 34, 92, 93, 91)
clean_oximetry(oximetry_data)
```

---

`create_xts`*Create an XTS Object from Resampled Signals*

---

**Description**

This function takes multiple signals and their corresponding sample rates, resamples the signals to the highest sample rate among them, and creates an xts (eXtensible Time Series) object with the resampled signals aligned according to a provided start time.

**Usage**

```
create_xts(signals, sample_rates, start_time)
```

**Arguments**

<code>signals</code>	A list of numeric vectors representing the signals. Each signal in the list should correspond to one sample rate in the ‘sample_rates’ argument.
<code>sample_rates</code>	A numeric vector containing the sample rates for each signal in ‘signals’. The length of ‘sample_rates’ must match the length of ‘signals’.
<code>start_time</code>	The start time for the xts object. This can be a character string or an object that can be converted to POSIXct. The time is assumed to be in UTC.

**Value**

An xts object containing the resampled signals, with each column representing one of the original signals, resampled to the highest sample rate among them. The xts object’s index starts from ‘start\_time’ and increments at a rate of 1 divided by the maximum sample rate.

**Examples**

```
signals <- list(rnorm(100), rnorm(100))
sample_rates <- c(1, 2)
start_time <- "2020-01-01 00:00:00"
xts_data <- create_xts(signals, sample_rates, start_time)
plot(xts_data)
```

---

detect\_apneic\_events *Detect Apneic Events in SpO2 Signal Data*

---

## Description

This function implements the algorithm described by Jung & Al in "Real-Time Automatic Apneic Event Detection Using Nocturnal Pulse Oximetry", 2018. It analyzes a given SpO2 signal to detect apneic events. It works by resampling the input signal and applying a series of checks to identify potential apnea instances. The algorithm uses a state machine with different blocks representing various stages of detection.

## Usage

```
detect_apneic_events(spo2, sRate)
```

## Arguments

spo2	A numeric vector representing the SpO2 signal data.
sRate	The original sampling rate of the SpO2 signal.

## Value

A list of numeric vectors. Each vector represents a detected apneic event, containing the start and end indices of the event in the resampled signal.

## References

Jung, D. W., Hwang, S. H., Cho, J. G., Choi, B. H., Baek, H. J., Lee, Y. J., Jeong, D.-U., & Park, K. S. (2018). Real-Time Automatic Apneic Event Detection Using Nocturnal Pulse Oximetry. In IEEE Transactions on Biomedical Engineering (Vol. 65, Issue 3, pp. 706–712). Institute of Electrical and Electronics Engineers (IEEE). <https://doi.org/10.1109/tbme.2017.2715405>

## Examples

```
# Example usage
spo2_sample <- c(98, 97, 96, 95, 94, 93, 92, 91, 90, 89, 88)
sample_rate <- 1 # Assuming 1 Hz sampling rate
detected_apneas <- detect_apneic_events(spo2_sample, sample_rate)
print(detected_apneas)
```

---

 detect\_rem

*Detection of Rapid-Eye Movements (REMs)*


---

### Description

Implements the algorithm detailed in Agarwal & Al. "Detection of Rapid-Eye Movements in Sleep Studies." This function processes electrooculography (EOG) signals to detect rapid-eye movements (REMs) characteristic of REM sleep, applying filters, artifact detection, and angle-based inclusion criteria.

### Usage

```
detect_rem(
    roc,
    loc,
    sRate,
    l = 0.5,
    art = 500,
    nip = 120,
    cc = -0.2,
    da = 45,
    dadiff = 15
)
```

### Arguments

roc	Right outer canthus EOG signal vector.
loc	Left outer canthus EOG signal vector.
sRate	Sampling rate of the EOG signals in Hz.
l	Window length in seconds for REM detection (default is 0.5).
art	Artifact threshold, max amplitude allowed in EOG signals to consider the data valid (default is 500).
nip	Negative Inflexion Point threshold for REM detection (default is 120).
cc	Correlation coefficient threshold for inclusion of a REM event. Negative correlation indicates potential REM (default is -0.2).
da	Desired angle for REM detection (default is 45 degrees).
dadiff	Acceptable deviation from the desired angle for one eye, if the other eye compensates with a larger deviation (default is 15 degrees).

### Details

The function processes the EOG signals by applying a band-pass Butterworth filter to isolate frequencies between 1 and 5 Hz, typical for REMs. It then computes the artifact measure and evaluates the signal for REM events based on the slope of the EOG signal segments, correlation between left

and right signals, and other criteria derived from the REM detection algorithm described by Agarwal et al. The function returns a list containing filtered EOG signals, artifact measures, and detected REM events with their characteristics and validity based on the algorithm's criteria.

### Value

A list with the following elements: - 'rocf': Filtered right outer canthus EOG signal. - 'locf': Filtered left outer canthus EOG signal. - 'block\_art': Maximum absolute amplitude in the EOG channels for the detection block, used for artifact measurement. - 'cpm': Product of inverted left and right EOG signals, part of REM detection criteria. - 'cn': Conditioned signal based on 'cpm', with values below a threshold set to 0. - 'crems': Data frame of candidate REMs with indices, characteristics, and validity flag. - 'rems': Subset of 'crems' containing only the valid REM events.

### References

Agarwal, R., Takeuchi, T., Laroche, S., & Gotman, J. (2005). Detection of Rapid-Eye Movements in Sleep Studies. *IEEE Transactions on Biomedical Engineering*, 52(8), 1390–1396. <https://doi.org/10.1109/TBME.2005.851511>

---

detect_rpeaks	<i>Detect R peaks in a raw ECG signal.</i>
---------------	--

---

### Description

'detect\_rpeaks' implements the first part of the Pan & Tompkins algorithms to detect R peaks from a raw ECG signal.

### Usage

```
detect_rpeaks(
  signal,
  sRate,
  lowcut = 0,
  highcut = 15,
  filter_order = 1,
  integration_window = 15,
  refractory = 200,
  return_index = FALSE
)
```

### Arguments

signal	Numerical vector of ECG signal.
sRate	ECG signal sample rate.
lowcut	Butterworth bandpass filter low cut value.
highcut	Butterworth bandpass filter high cut value.
filter_order	Butterworth bandpass filter order value.

integration\_window      Convolution window size.  
 refractory              Minimal space between peaks in milliseconds.  
 return\_index          If TRUE, the index for each R peak is returned instead of the timing.

### Value

A numeric vector of detected R peaks, expressed in seconds\* from the start of the signal. This vector can be used in RHRV using 'RHRV::LoadBeatVector()'.

\*(or samples if return\_index is TRUE)

### References

Pan, Jiapu, and Willis J. Tompkins. "A real-time QRS detection algorithm." IEEE Trans. Biomed. Eng 32, no. 3 (1985): 230-236.

### Examples

```
tryCatch({
  path <- paste0(tempdir(),"rec_1.dat")
  download.file("https://rsleep.org/data/rec_1.sdat",path)
  ecg <- readBin(path,integer(),500*30)
  peaks <- detect_rpeaks(ecg, sRate = 500)
  unlink(path)
  print(peaks)
  ecg.df <- data.frame(ECG = ecg,Seconds = c(1:length(ecg))/500)
  library(ggplot2)
  ggplot(ecg.df,aes(x = Seconds,y = ECG)) +
    geom_line() +
    theme_bw() +
    geom_vline(
      data.frame(p = peaks),
      mapping = aes(xintercept = p),
      linetype="dashed",
      color = "red")
}, error = function(e) {
  print("Error executing this example, check your internet connection.")
})
```

---

epochs	<i>Split signals into consecutive, non-overlapping epochs according to an events dataframe or an epoch duration.</i>
--------	--

---

### Description

Split long signals into a list of consecutive epochs according to an events dataframe or an epoch duration.

**Usage**

```
epochs(
  signals,
  sRates,
  resample = max(sRates),
  epoch = 30,
  startTime = 0,
  padding = 0
)
```

**Arguments**

signals	A list of numeric vectors containing signals, or a single vector containing one signal.
sRates	A vector or list of integer values of the signals sample rates.
resample	The sample rate to resample all signals. Defaults to the max of the provided sample rates.
epoch	Epochs reference. Can be an events dataframe or the number of seconds of each epoch Defaults to 30.
startTime	The start timestamp of the signal, used to join events to epoch.
padding	Number of previous and next epochs to pad the current epoch with. This functionality is mostly used to enrich deep learning datasets. Defaults to 0.

**Value**

A list of signal chunks

**Examples**

```
epochs(list(rep(c(1,2,3,4),100),rep(c(5,6,7,8),100)),4,4,1,padding = 2)
```

---

hypnogram	<i>Filter and reorder an events dataframe or a hypnodensity to keep only sleep stages related-events.</i>
-----------	---

---

**Description**

Remove non-sleep stages events and reorder dataframe rows using the begin column.

**Usage**

```
hypnogram(
  events,
  labels = c("N3", "N2", "N1", "REM", "AWA"),
  startTime = 946681200,
  epoch_duration = 30,
  plot = FALSE
)
```



**Arguments**

events	Events dataframe. Dataframe must have begin (POSIXt), end (POSIXt) and event
labels	Sleep stages labels. Defaults to c("N3", "N2", "N1", "REM", "AWA").
startTime	Hypnogram start time. Used when a hypnodensity dataframe is passed as events. Defaults to 946681200.
epoch_duration	Epoch duration in seconds. Used when a hypnodensity dataframe is passed as events. Defaults to 30.
plot	Plot the hypnogram or in not using ggplot2.

**Value**

Hypnogram dataframe or plot.

**Examples**

```
tryCatch({
  fpath <- paste0(tempdir(), "/15012016HD.csv")

  download.file("https://rsleep.org/data/15012016HD.csv", fpath, method="curl")

  events <- read_events_nocturnal(fpath)

  unlink(fpath)

  hypnogram(events)
}, error = function(e) {
  print("Error executing this example, check your internet connection.")
})
```

---

normalize_cycles	<i>Normalize sleep cycles scored on Nocturnal software from start and stop flags to unique events.</i>
------------------	--

---

**Description**

Normalize sleep cycles scored on Nocturnal software from start and stop flags to unique events.

**Usage**

```
normalize_cycles(events)
```

**Arguments**

events	Events dataframe. Dataframe must have begin (POSIXt), end (POSIXt) and event. Cycles flags must be named Activity-CLASSICstart, Activity-BNstart, Activity-BNend, Activity-REMstart, Activity-REMend, Activity-ENstart or Activity-ENend.
--------	---

**Examples**

```
cycles <- data.frame(event = c("Activity-CLASSICstart", "Activity-CLASSICend"))
cycles$begin <- as.POSIXct(c("2016-01-16 01:13:30", "2016-01-16 01:15:30"))
cycles$end <- as.POSIXct(c("2016-01-16 01:13:30", "2016-01-16 01:15:30"))
normalize_cycles(cycles)
```

---

periods	<i>Get a dataframe of sleep periods from a hypnogram, continuous or by stages.</i>
---------	--

---

**Description**

Get a dataframe of sleep periods from a hypnogram, continuous or by stages.

**Usage**

```
periods(
  hypnogram,
  mode = "continuous",
  stages = c("N1", "N2", "N3", "N4", "REM")
)
```

**Arguments**

hypnogram	A hypnogram dataframe. Dataframe must contain begin (POSIXt), end (POSIXt) and event (character) columns.
mode	Period mode. "continuous" computes periods of N1, N2, N3 or REM sleep, regardless of stage. "stages" computes periods of sleep by stage.
stages	Stages to include in periods. Defaults to 'c("N1", "N2", "N3", "N4", "REM")'.

**Value**

A dataframe of periods with their begin and stop times, duration and stages for stage mode.

**Examples**

```
tryCatch({
  library(ggplot2)

  download.file(
    "https://rsleep.org/data/hypnodensity.csv",
    "hypnodensity.csv")

  hypnodensity <- read.csv2("hypnodensity.csv")

  unlink("hypnodensity.csv")

  events <- hypnogram(hypnodensity)
```

```
periods_continuous <- periods(events, mode = "continuous")

ggplot(periods_continuous, aes(x=duration)) + geom_histogram(bins = 30)

periods_stages <- periods(events, mode = "stages")

ggplot(periods_stages, aes(x=event,y=duration,color=event)) + geom_boxplot()
}, error = function(e) {
  print("Error executing this example, check your internet connection.")
})
```

---

plot_event	<i>Highlight a scored event over a signal.</i>
------------	--

---

### Description

Highlight a scored event over a signal.

### Usage

```
plot_event(signal, sRate, sig_start, event_start, event_end, window = 10)
```

### Arguments

signal	The signal vector.
sRate	Sample rate of the signal.
sig_start	Date-Time value of the signal start.
event_start	Date-Time value of the event start.
event_end	Date-Time value of the event end.
window	Number of seconds of signal to plot before, and after.

### Value

A plot of the highlighted event over the signal.

---

plot\_hypnodensity      *Plot a hypnodensity graph.*

---

### Description

Plot a hypnodensity graph using 'ggplot2'. Hypnodensity can be read from file or returned by the 'score\_stages\_edf' function.

### Usage

```
plot_hypnodensity(  
  hypnodensity,  
  stages = c("AWA", "REM", "N1", "N2", "N3"),  
  colors = c("#5BBCD6", "#FF0000", "#00A08A", "#F2AD00", "#F98400")  
)
```

### Arguments

hypnodensity      A hypnodensity dataframe as returned by the 'score\_stages\_edf' function.  
stages              Vector of stages labels to plot.  
colors              Vector of colors to use.

### Value

A 'ggplot2' hypnodensity graph.

### References

Stephansen, J.B., Olesen, A.N., Olsen, M., Ambati, A., Leary, E.B., Moore, H.E., Carrillo, O., Lin, L., Han, F., Yan, H. and Sun, Y.L., 2018. Neural network analysis of sleep stages enables efficient diagnosis of narcolepsy. Nature communications, 9(1), p.5229.

### Examples

```
tryCatch({  
  download.file("https://rsleep.org/data/hypnodensity.csv", "hypnodensity.csv")  
  
  hypnodensity <- read.csv2("hypnodensity.csv")  
  
  unlink("hypnodensity.csv")  
  
  plot_hypnodensity(hypnodensity)  
}, error = function(e) {  
  print("Error executing this example, check your internet connection.")  
})
```

---

plot\_hypnogram            *Plot a hypnogram from an events dataframe.*

---

**Description**

Plot a hypnogram from an events dataframe.

**Usage**

```
plot_hypnogram(events, labels = c("N3", "N2", "N1", "REM", "AWA"))
```

**Arguments**

events            Events dataframe. Dataframe must have begin (POSIXt), end (POSIXt) and event

labels            Sleep stages labels. Defaults to c("N3", "N2", "N1", "REM", "AWA").

**Value**

a ggplot object.

**Examples**

```
hypnogram <- data.frame(begin = as.POSIXlt(
  c(1536967800, 1536967830, 1536967860), origin = "1970-01-01"))
hypnogram$end <- as.POSIXlt(c(1536967830, 1536967860, 1536967890),
  origin = "1970-01-01")
hypnogram$event = c("N3", "N3", "REM")
plot_hypnogram(hypnogram)
```

---

psm                      *Power spectral density using adaptive sine multitaper.*

---

**Description**

Power spectral density using adaptive sine multitaper.

**Usage**

```
psm(x, sRate, length = 0, show = TRUE)
```

**Arguments**

x	Signal vector.
sRate	Sample rate of the signal.
length	periodogram resolution. 0 default to not resize.
show	todo

**Value**

peridodogram plotted or raw.

**References**

Barbour, A. J. and R. L. Parker (2014), psd: Adaptive, sine multitaper power spectral density estimation for R, Computers & Geosciences, Volume 63, February 2014, Pages 1-8, ISSN 0098-3004, <http://dx.doi.org/10.1016/j.cageo.2013.09.015>

**Examples**

```
x <- sin(c(1:10000))
psd <- psm(x, 200, 100)
head(psd)
```

---

pwelch

*Power spectral density using Welch's method.*

---

**Description**

Power spectral density using Welch's method.

**Usage**

```
pwelch(x, sRate, points = 0, overlap = 0, padding = 0, show = TRUE)
```

**Arguments**

x	Signal vector.
sRate	Sample rate of the signal.
points	todo
overlap	todo
padding	todo
show	todo

**Value**

peridodogram plotted or raw

## References

Welch, P. "The Use of Fast Fourier Transform for the Estimation of Power Spectra: A Method Based on Time Averaging over Short, Modified Periodograms." IEEE Transactions on Audio and Electroacoustics 15, no. 2 (June 1967): 70–73. <https://doi.org/10.1109/TAU.1967.1161901>.

## Examples

```
x <- sin(c(1:10000))
psd <- pwelch(sin(c(1:10000)), 200)
head(psd)
```

---

```
read_events_compumedics
```

*Read a stages export from Compumedics software in .txt format.*

---

## Description

Read a stages export from Compumedics software in .txt format.

## Usage

```
read_events_compumedics(  
  txt,  
  startTime = as.POSIXlt("2000-01-01"),  
  labels = c(AWA = 0, N1 = 1, N2 = 2, N3 = 3, REM = 5)  
)
```

## Arguments

txt	txt file path.
startTime	Character string or date object of the hypnogram start.
labels	Labels and values as a named list. Defaults to c("AWA" = 0, "N1" = 1, "N2" = 2, "N3" = 3, "REM" = 5).

## Value

A dataframe of stages.

---

read\_events\_ndb      *Read events from a Resmed Noxturnal .ndb file.*

---

**Description**

Read events from a Resmed Noxturnal .ndb file.

**Usage**

```
read_events_ndb(data_file)
```

**Arguments**

data\_file      .ndb file path.

**Value**

An events dataframe.

---

read\_events\_noxturnal      *Read a Noxturnal events file (Unicode CSV format)*

---

**Description**

Read a Noxturnal events file (Unicode CSV format)

**Usage**

```
read_events_noxturnal(dir)
```

**Arguments**

dir              Noxturnal events file path.

**Value**

A dataframe of scored events.



---

read\_events\_profusion *Read a annotation file from Compumedics Profusion software in XML format.*

---

**Description**

Read a annotation file from Compumedics Profusion software in XML format.

**Usage**

```
read_events_profusion(xml, startTime = as.POSIXlt("1970-01-01 00:00:00"))
```

**Arguments**

xml	XML file path.
startTime	Character string or date object of the hypnogram start.

**Value**

A dataframe of stages and events.

---

read\_events\_sleepedx *Read a SleepEDFX events file EDF+*

---

**Description**

Read a SleepEDFX events file EDF+

**Usage**

```
read_events_sleepedx(dir, update = TRUE)
```

**Arguments**

dir	EDF+ path
update	merge N3 and N4 or not

**Value**

A dataframe of scored events.

---

read_mdf	<i>Read a Morpheo Data Format (MDF) directory to a list.</i>
----------	--

---

**Description**

Read a Morpheo Data Format (MDF) directory to a list.

**Usage**

```
read_mdf(mdfPath, channels = c(NA), metadata = TRUE)
```

**Arguments**

mdfPath	character. MDF path.
channels	character. Channels to read.
metadata	boolean. Read or not the metadata.

**Value**

A list.

**References**

P. Bouchequet, D. Jin, G. Solelhac, M. Chennaoui, D. Leger, "Morpheo Data Format (MDF), un nouveau format de données simple, robuste et performant pour stocker et analyser les enregistrements de sommeil", *Médecine du Sommeil*, vol. 15, n 1, p. 48/49, march 2018.

---

schwabedal2018	<i>Automated Classification of Sleep Stages in Mice with Deep Learning model implementation in Keras.</i>
----------------	---

---

**Description**

Model inspired by the article "Automated Classification of Sleep Stages and EEG Artifacts in Mice with Deep Learning". Implemented using Keras. Adapted to use minimum 2 channels and to not score artifact epochs.

**Usage**

```
schwabedal2018(channels = 2, samples = 8000)
```

**Arguments**

channels	Number of channels in each input.
samples	Number of samples in each channel.

**Value**

A Keras sequential model.

**References**

Schwabedal, Justus T. C., Daniel Sippel, Moritz D. Brandt, and Stephan Bialonski. "Automated Classification of Sleep Stages and EEG Artifacts in Mice with Deep Learning." ArXiv:1809.08443 [Cs, q-Bio], September 22, 2018. <http://arxiv.org/abs/1809.08443>.

---

score_mice	<i>Score mice sleep from European Data Format (EDF) files.</i>
------------	--

---

**Description**

Score mice sleep from European Data Format (EDF) files.

**Usage**

```
score_mice(edf, model, verbose = TRUE)
```

**Arguments**

edf	Character. European Data Format (EDF) file path.
model	model
verbose	Boolean. Display or not status messages.

**Value**

A dataframe containing predicted hypnodensity values of the record.

---

score_psg	<i>Score 30 seconds epochs from European Data Format (EDF) files.</i>
-----------	---

---

**Description**

Score 30 seconds epochs from European Data Format (EDF) files.

**Usage**

```
score_psg(
  edf,
  channels = c("C3-M2", "C4-M1", "O1-M2", "E1-M2", "E2-M1", "1-2"),
  model = chambon2018(6, 3 * 30 * 70),
  verbose = TRUE
)
```

**Arguments**

<code>edf</code>	Character. European Data Format (EDF) file path.
<code>channels</code>	A vector containing the channels names if names differ from <code>'c("C3-M2","C4-M1","O1-M2","E1-M2","E2-M1","1-2")'</code> .
<code>model</code>	The Keras model.
<code>verbose</code>	Boolean. Display or not status messages.

**Value**

A dataframe containing predicted hypnodensity values of the record.

**References**

- Chambon, S., Galtier, M., Arnal, P., Wainrib, G. and Gramfort, A. (2018) A Deep Learning Architecture for Temporal Sleep Stage Classification Using Multivariate and Multimodal Time Series. *IEEE Trans. on Neural Systems and Rehabilitation Engineering* 26:(758-769).
- Kemp, B., Värrri, A., Rosa, A.C., Nielsen, K.D. and Gade, J., 1992. A simple format for exchange of digitized polygraphic recordings. *Electroencephalography and clinical neurophysiology*, 82(5), pp.391-393.

---

segmentation

*Split signals into consecutive, overlapping segments.*

---

**Description**

Split signals into consecutive, overlapping segments.

**Usage**

```
segmentation(
  signals,
  sRates,
  segments_size = 10,
  step = 1,
  padding = 0,
  resample = max(sRates),
  return_index = FALSE
)
```

**Arguments**

<code>signals</code>	A list of numeric vectors containing signals, or a single vector containing one signal.
<code>sRates</code>	A vector or list of integer values of the signals sample rates.
<code>segments_size</code>	The size of segments, in seconds.

step	The step between segments, in seconds.
padding	umber of previous and next epochs to pad the current epoch with. Defaults to 0.
resample	The sample rate to resample all signals. Defaults to to the max of the provided sample rates.
return_index	If TRUE, the index of segments is returned instead of the segments.

**Value**

A matrix of segments.

**References**

Choi SH, Yoon H, Kim HS, et al. Real-time apnea-hypopnea event detection during sleep by convolutional neural networks. *Computers in Biology and Medicine*. 2018;100:123-131.

**Examples**

```
computed_segments = segmentation(
  signals = list(c(sin(1:1000)),c(cos(1:1000))),
  sRates = c(1, 1),
  segments_size = 5,
  resample = 1)
dim(computed_segments)
plot(computed_segments[1,,1], type = "l")
plot(computed_segments[2,,1], type = "l")
```

---

smooth_hypnogram	<i>Smooth hypnogram epoch, simulating human scorers behaviour.</i>
------------------	--

---

**Description**

Smooth hypnograms epoch, simulating human scorers behaviour.

**Usage**

```
smooth_hypnogram(hypnogram, event = "N2", neighbors = "REM", count = 2)
```

**Arguments**

hypnogram	A hypnogram dataframe.
event	Central stage label.
neighbors	Extremities stages labels.
count	Number of consecutive central stages.

**Value**

A hypnogram dataframe.

## References

Liang, Sheng-Fu, Chin-En Kuo, Yu-Han Hu, Yu-Hsiang Pan, and Yung-Hung Wang. "Automatic stage scoring of single-channel sleep EEG by using multiscale entropy and autoregressive models." *IEEE Transactions on Instrumentation and Measurement* 61, no. 6 (2012): 1649-1657.

## Examples

```
hypnogram <- data.frame(begin = as.POSIXlt(
  c(1536967800,1536967830,1536967860),origin = "1970-01-01"))
hypnogram$end <- as.POSIXlt(c(1536967830,1536967860,1536967890),
  origin = "1970-01-01")
hypnogram$event = c("REM", "N2", "REM")
smooth_hypnogram(hypnogram, "N2", "REM", 1)
```

---

smooth_liang2012	<i>Smooth hypnogram according to the 11 rules described by Liang &amp; Al.</i>
------------------	--

---

## Description

Smooth hypnogram according to the 11 rules described by Liang & Al.

## Usage

```
smooth_liang2012(hypnogram)
```

## Arguments

hypnogram      A hypnogram dataframe.

## Value

A smoothed hypnogram dataframe.

## References

Liang, Sheng-Fu, Chin-En Kuo, Yu-Han Hu, and Yu-Shian Cheng. "A Rule-Based Automatic Sleep Staging Method." *Journal of Neuroscience Methods* 205, no. 1 (March 2012): 169–76. <https://doi.org/10.1016/j.jneumeth.2011.12.022>.

---

spectrogram *Plot the spectrogram of signal.*

---

### Description

‘spectrogram’ resamples signal and use the ‘specgram’ function from the ‘signal’ library to compute the spectrogram. Results resolution can be then reduced to quickly plot large signals.

### Usage

```
spectrogram(
  signal,
  sRate,
  maxFreq = 25,
  n = 1024,
  window = n,
  overlap = 0,
  cols = c(rep("#3B9AB2", 9), "#78B7C5", "#EBCC2A", "#E1AF00", rep("#F21A00", 6)),
  freq = 4,
  plot = TRUE,
  startTime = as.POSIXct("1970/01/01 00:00:00")
)
```

### Arguments

signal	Numerical vector of the signal.
sRate	Signal sample rate in Hertz.
maxFreq	Maximal frequency to plot in Hertz. Signal will be resampled at maxFreq*2 sample rate.
n	The size of the Fourier transform window.
window	Shape of the fourier transform window, defaults to n.
overlap	Overlap with previous window, defaults to 0.
cols	Color scale used for the underlying plot function.
freq	Aggregate frequency used to lower spectrogram resolution. Defaults to 4.
plot	Boolean, plot or not the spectrogram.
startTime	Posixct of the signal start. Adjust the x axis labels accordingly.

### Value

A spectrogram.

### Examples

```
library(signal)
spectrogram(chirp(seq(-2, 15, by = 0.001), 400, 10, 100, 'quadratic'),20,n=1024)
```

---

stages_stats	<i>Get stages related statistics in a named vector.</i>
--------------	---

---

**Description**

stages\_stats computes stages related statistics.

**Usage**

```
stages_stats(e)
```

**Arguments**

e Events dataframe. Dataframe must have begin (POSIXt), end (POSIXt) and event (character) columns.

**Value**

stages vector

**Examples**

```
e <- data.frame(begin = as.POSIXlt(seq(from = 0, to = 30*10, by = 30),origin = "1970-01-01"))
e$end <- as.POSIXlt(seq(from = 30, to = 30*11, by = 30), origin = "1970-01-01")
e$event = c("AWA", "N1", "N2", "N3", "N3", "REM", "N2", "REM", "N2", "REM", "AWA")
stages_stats(e)
```

---

train_batches	<i>Trains a model from files batches.</i>
---------------	---

---

**Description**

Trains a model from files batches.

**Usage**

```
train_batches(model, batches, epochs = 10)
```

**Arguments**

model Keras model.  
 batches Character vector of batches files.  
 epochs Integer. Number of epochs to train the model.

**Value**

A trained and serialized Keras model.



---

transitions	<i>Count and format stages transitions.</i>
-------------	---

---

### Description

Count and format stages transitions.

### Usage

```
transitions(  
  hypnogram,  
  stages = c("AWA", "REM", "N1", "N2", "N3", "NREM"),  
  format = "vector"  
)
```

### Arguments

hypnogram	A hypnogram dataframe. Dataframe must contain begin (POSIXt), end (POSIXt) and event (character) columns.
stages	Stages to include in transitions Defaults to c("N1", "N2", "N3", "N4", "REM").
format	Set the return format. 'vector', 'dataframe' or 'heatmap'.

### Value

Count of stages transitions in selected format.

### References

Swihart BJ, Punjabi NM, Crainiceanu CM. Modeling sleep fragmentation in sleep hypnograms: An instance of fast, scalable discrete-state, discrete-time analyses. *Comput Stat Data Anal.* 2015 Sep;89:1-11. doi: 10.1016/j.csda.2015.03.001. PMID: 27182097; PMCID: PMC4865264.

### Examples

```
tryCatch({  
  download.file("https://rsleep.org/data/hypnodensity.csv", "hypnodensity.csv")  
  
  hypnodensity <- read.csv2("hypnodensity.csv")  
  
  unlink("hypnodensity.csv")  
  
  events <- hypnogram(hypnodensity)  
  
  transitions(events)  
  
  transitions(events, format = "dataframe")  
  
  transitions(events, format = "heatmap")
```

```

# 3 Dimensions sleep transitions
levels(events$event)[levels(events$event)=="N1"] <- "NREM"
levels(events$event)[levels(events$event)=="N2"] <- "NREM"
levels(events$event)[levels(events$event)=="N3"] <- "NREM"

round(
  transitions(
    events,
    format = "dataframe")/(
    sum(transitions(events))*100,2)
), error = function(e) {
  print("Error executing this example, check your internet connection.")
})

```

---

tst90	<i>Compute TST90, the percentage of time during sleep with an oxygen saturation below 90.</i>
-------	---

---

### Description

Compute TST90, the percentage of time during sleep with an oxygen saturation below 90.

### Usage

```
tst90(spo2_signal, sRate, startTime, hypnogram)
```

### Arguments

spo2_signal	The SpO2 signal vector.
sRate	The SpO2 signal vector sample rate.
startTime	The SpO2 signal start time.
hypnogram	Events dataframe containing hypnogram.

---

write_batches_mice	<i>Write batches from mice records</i>
--------------------	--

---

### Description

Write batches from mice records

**Usage**

```

write_batches_mice(
    records,
    events,
    batches_path = "./",
    batch_size = 128,
    classes_nb = 3,
    padding = 2,
    resample = 400,
    verbose = TRUE
)

```

**Arguments**

records	Character. Records paths
events	List of events
batches_path	Path to write batches
batch_size	size of each batch
classes_nb	number of classes
padding	consecutive epochs to add
resample	resample rate
verbose	Boolean. Display or not status messages.

---

write_batches_psg	<i>Generates files batches from PSG data.</i>
-------------------	---

---

**Description**

Generates train batches from PSG data to be used by the 'train\_batches()' function.

**Usage**

```

write_batches_psg(
    records,
    events,
    batches_path = tempdir(),
    channels = c("C3-M2", "C4-M1", "O1-M2", "E1-M2", "E2-M1", "1-2"),
    resample = 70,
    padding = 1,
    batches_size = 1024,
    verbose = TRUE
)

```

**Arguments**

records	Character vector of EDF files paths to be included in the train batches.
events	List of events dataframes containing hypnograms corresponding to EDF records in 'records' parameter.
batches_path	Character. Path where batches files will be saved.
channels	Character vector. Channels labels to include in the dataset.
resample	Integer. Sample rate to resample selected signals.
padding	Epochs added before and after each epoch.
batches_size	Number of epochs in each batch file.
verbose	Boolean, display status messages or not.

**References**

Chambon, S., Galtier, M., Arnal, P., Wainrib, G. and Gramfort, A. (2018) A Deep Learning Architecture for Temporal Sleep Stage Classification Using Multivariate and Multimodal Time Series. *IEEE Trans. on Neural Systems and Rehabilitation Engineering* 26:(758-769).

---

write_channel	<i>Write a timeserie to disk using Morpheo Data Format (MDF) guidelines.</i>
---------------	--

---

**Description**

Write a timeserie to disk using Morpheo Data Format (MDF) guidelines.

**Usage**

```
write_channel(channel, signals, headers, mdfPath, endian = .Platform$endian)
```

**Arguments**

channel	character. Channel name.
signals	list. European Data Format (EDF) signals list.
headers	list. European Data Format (EDF) file headers.
mdfPath	character. Morpheo Data Format (MDF) directory path.
endian	character. Endianess. "big" or "little". Defaults to platform endian.

**References**

P. Bouchequet, D. Jin, G. Solelhac, M. Chennaoui, D. Leger, "Morpheo Data Format (MDF), un nouveau format de données simple, robuste et performant pour stocker et analyser les enregistrements de sommeil", *Médecine du Sommeil*, vol. 15, n 1, p. 48-49, march 2018.

---

```
write_hypnogram_compumedics
```

*Write a XML file containing scored stages for Compumedics software.*

---

### Description

Write a XML file containing scored stages for Compumedics software.

### Usage

```
write_hypnogram_compumedics(hypnogram, filename)
```

### Arguments

hypnogram	A rsleep hypnogram dataframe.
filename	character File name to write on disk.

---

```
write_mdf
```

*Write a European Data Format (EDF) record file to disk using Morpheo Data Format (MDF) guidelines*

---

### Description

Write a European Data Format (EDF) record file to disk using Morpheo Data Format (MDF) guidelines. Target directory is erased if it already exists. Signals are stored in binary file, events and metadata in JavaScript Object Notation (JSON) files.

### Usage

```
write_mdf(
  edfPath,
  mdfPath,
  channels = c(NA),
  events = c(),
  endian = .Platform$endian
)
```

### Arguments

edfPath	character. European Data Format (EDF) file path.
mdfPath	character. Morpheo Data Format (MDF) directory path.
channels	character. Vector of channels labels to write.
events	dataframe. Events dataframe to write. Events dataframe. Dataframe must contain begin (POSIXt), end (POSIXt) and event (character) columns.
endian	character. Endianess. "big" or "little". Defaults to platform endian.

**References**

P. Bouchequet, D. Jin, G. Solelhac, M. Chennaoui, D. Leger, "Morpheo Data Format (MDF), un nouveau format de données simple, robuste et performant pour stocker et analyser les enregistrements de sommeil", *Médecine du Sommeil*, vol. 15, n 1, p. 48/49, march 2018.

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